



Finanziato  
dall'Unione europea  
NextGenerationEU



Ministero  
dell'Università  
e della Ricerca



Italiadomani  
PIANO NAZIONALE  
DI RIPRESA E RESILIENZA



109° CONGRESSO NAZIONALE

Società Italiana di Fisica

# Morpho-mechanics of collagen superstructures revealed by Brillouin-Raman microspectroscopy

**Silvia Caponi<sup>1</sup>, Maurizio Mattarelli<sup>1,2</sup>, Daniele Fioretto**

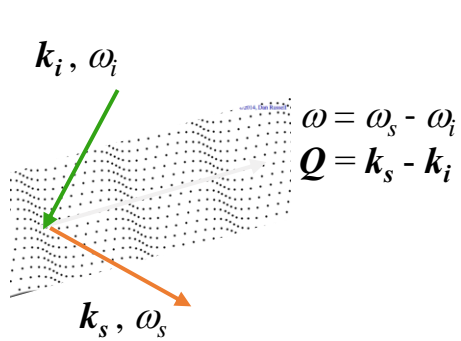
*<sup>1</sup> Istituto Officina dei Materiali, (IOM-CNR), Unit of Perugia*

*<sup>2</sup> Department of Physics and Geology, University of Perugia, 06123 Perugia - Italy*

# Brillouin

thermally activated acoustic waves

*Mechanical properties*

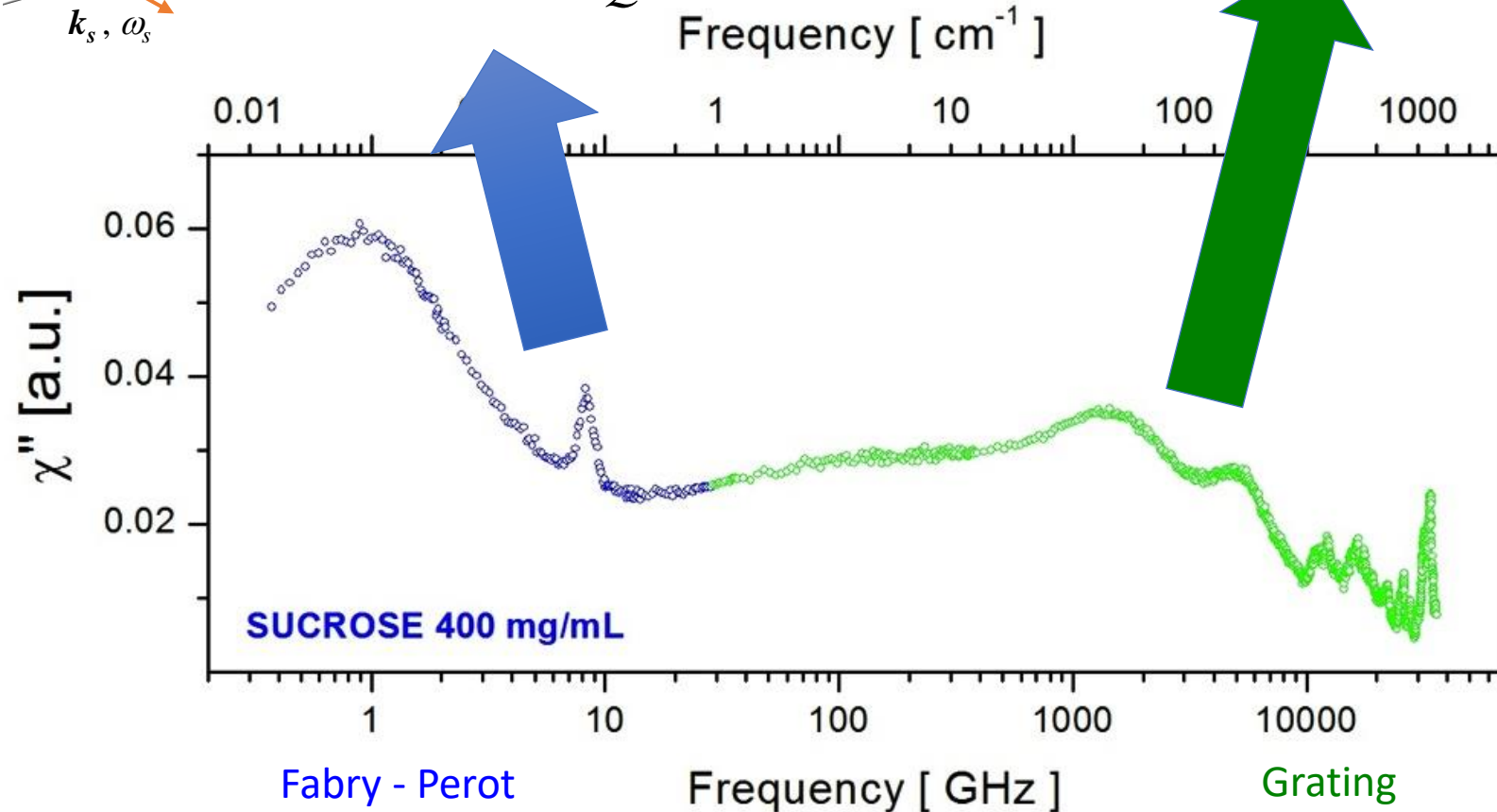
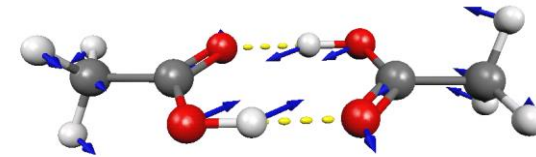


$$M = r \frac{W^2}{Q^2}$$
$$h_L = r \frac{G}{Q^2}$$

# Raman

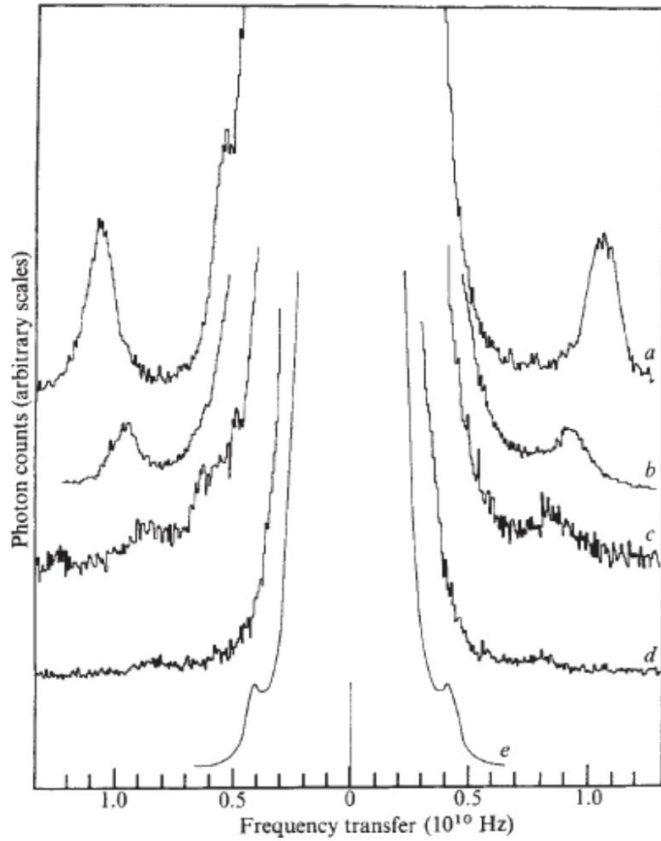
vibrational modes of molecules

*Chemical properties - composition, structure*

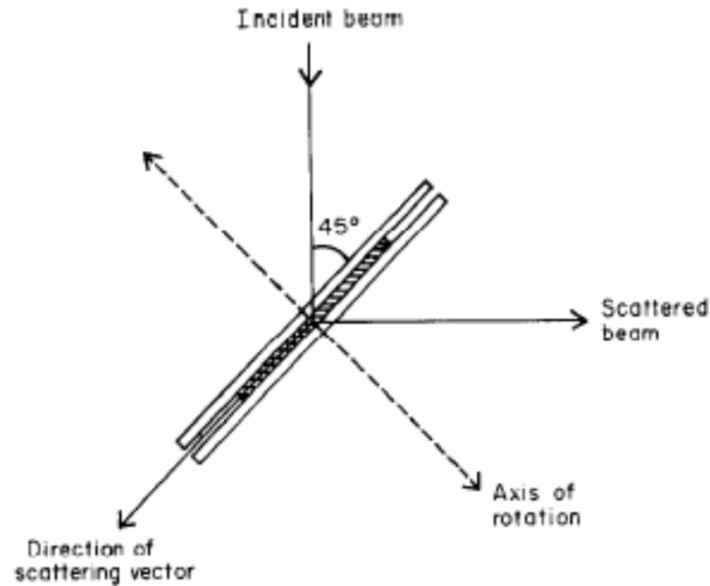


# First biological applications of Brillouin scattering

Rat tail tendon collagen fibres



R Harley et al. Nature 1977



Elastic constant	Dry collagen (density 1.35 g/cm <sup>3</sup> )	Native collagen (density 1.12 g/cm <sup>3</sup> )
$c_{11}$	17.9 GN m <sup>-2</sup>	7.8 GN m <sup>-2</sup>
$c_{12}$	11.7 GN m <sup>-2</sup>	4.0 GN m <sup>-2</sup>
$c_{44}$	3.3 GN m <sup>-2</sup>	---
$c_{13}$	5.1 GN m <sup>-2</sup>	---
$c_{23}$	7.1 GN m <sup>-2</sup>	---

$$E_{\parallel} = 11.9 \text{ GN m}^{-2} \quad \sigma_{13} = 0.42$$

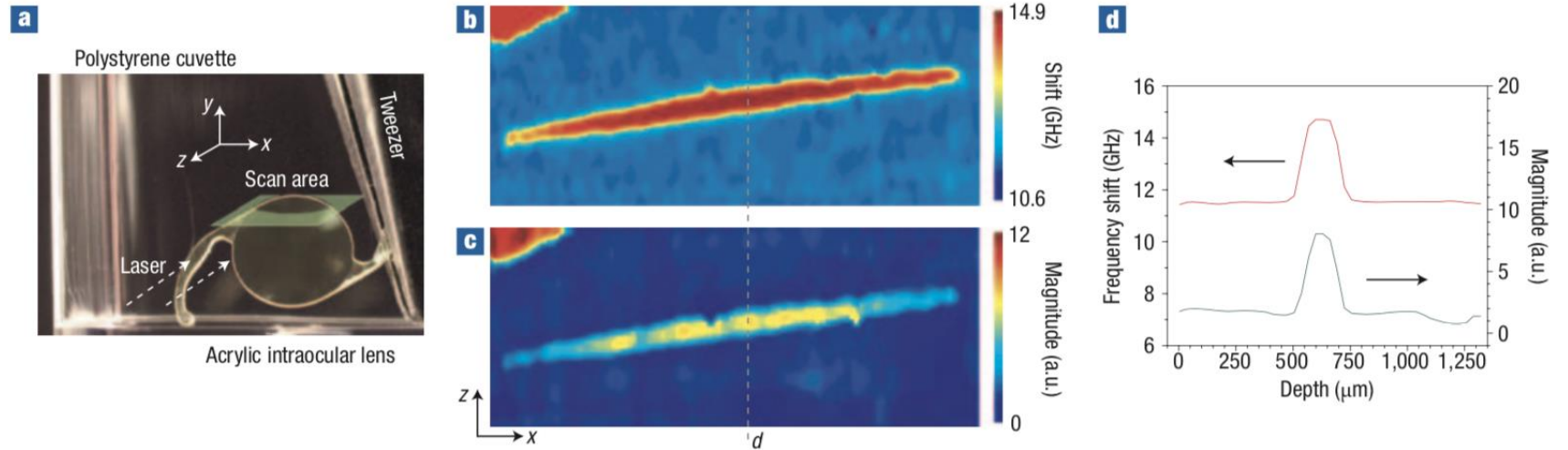
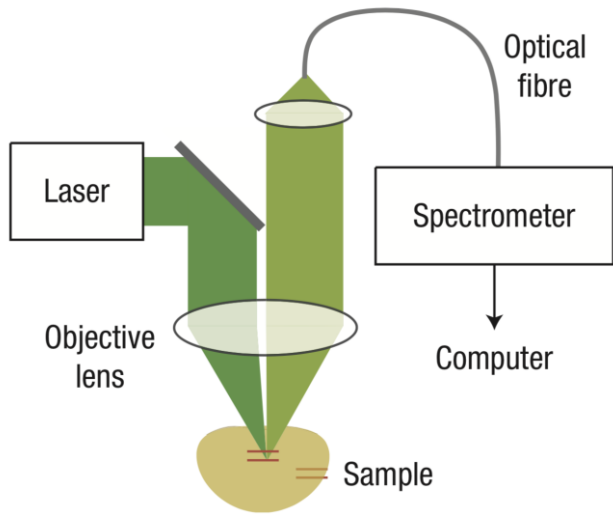
$$E_{\perp} = 8.3 \text{ GN m}^{-2} \quad \sigma_{12} = 0.26$$

$$G = 3.3 \text{ GN m}^{-2}$$

S Cusack & A Miller J. Mol. Biol. 1979  
EMBL Grenoble

# Brillouin meets Confocal Microscopy: micro-Brillouin imaging.

G. Scarcelli, S.H. Yun, Nature Photonics, 2, 39 (2007)

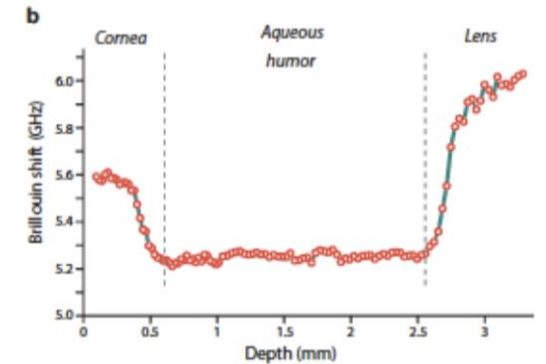
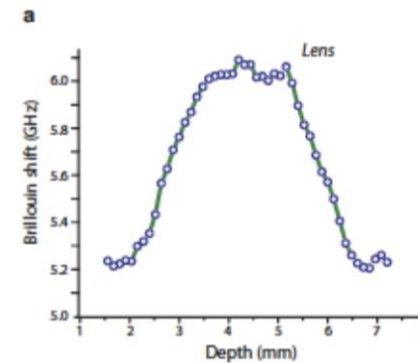
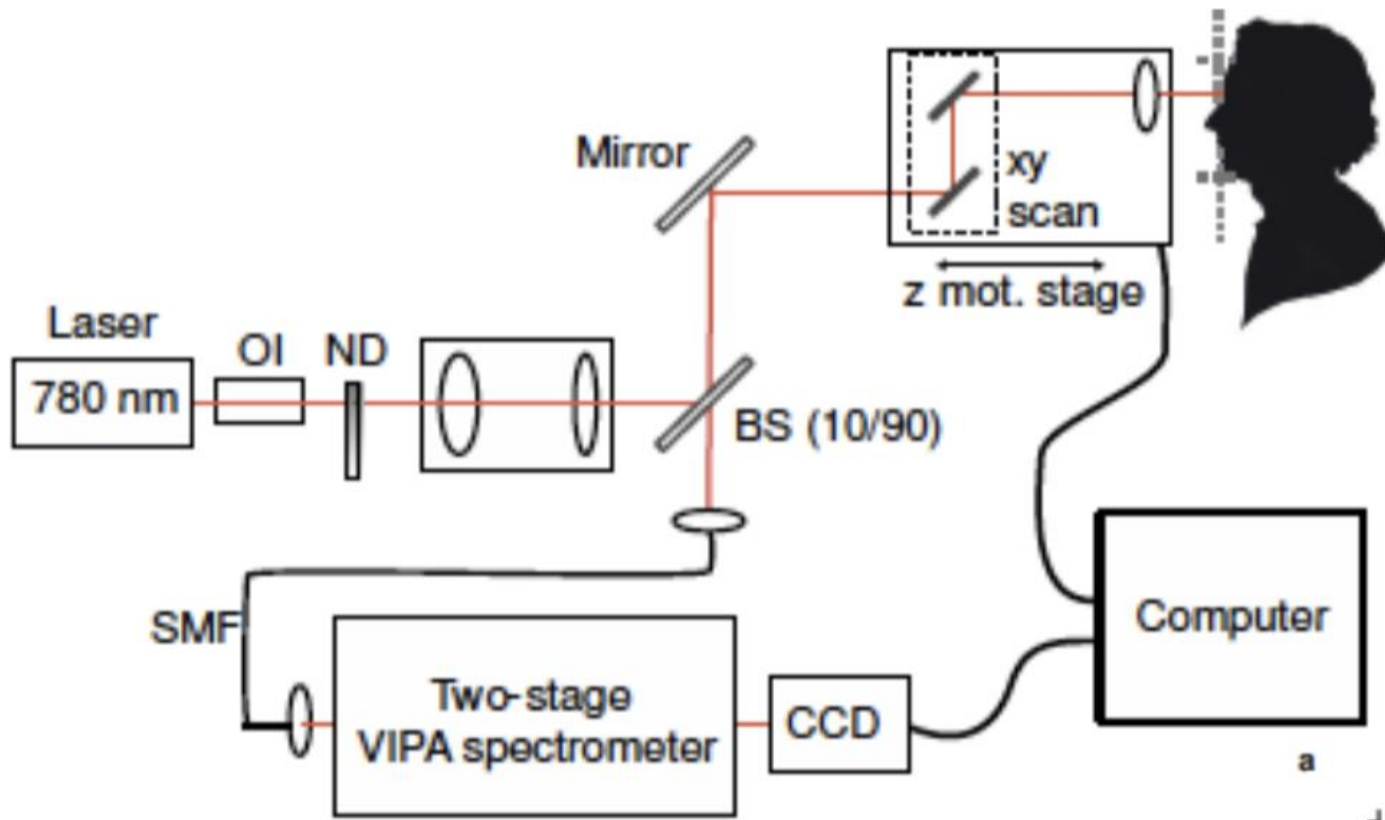


**Figure 3** Cross-sectional Brillouin image of an intraocular lens. **a**, Picture of the sample used. To visualize the outline of the lens clearly, the picture was taken before filling the cuvette with index-matching viscous polymer. The imaged area is 3.2 mm ( $x$ )  $\times$  1.3 mm ( $z$ ). **b**, Image based on measured frequency shifts, corresponding to a cross-sectional map of elastic modulus. **c**, Image created by using Brillouin scattering magnitudes as contrast. **d**, Representative cross-sectional line profiles taken along the dotted line in **b** and **c**. Arrows indicate which  $y$  axis scale applies.

# Brillouin meets Confocal Microscopy: micro-Brillouin imaging

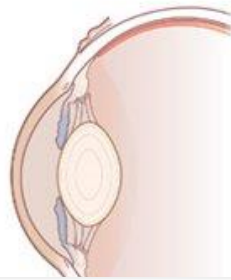
## First *in vivo* application to human eye

G. Scarcelli, S.H. Yun, Opt. Express, 2012

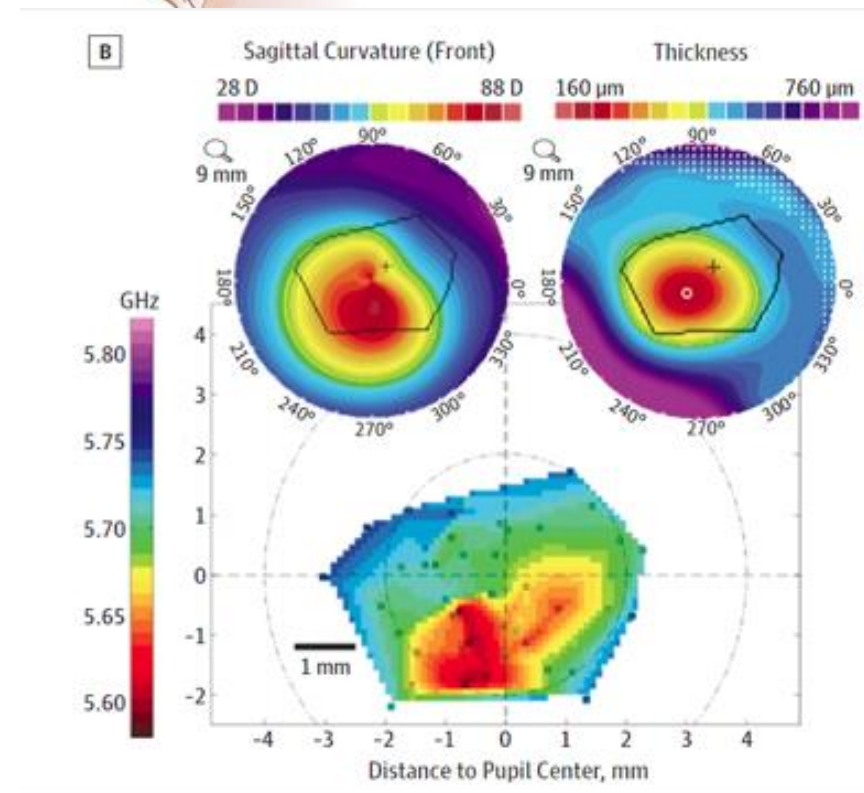
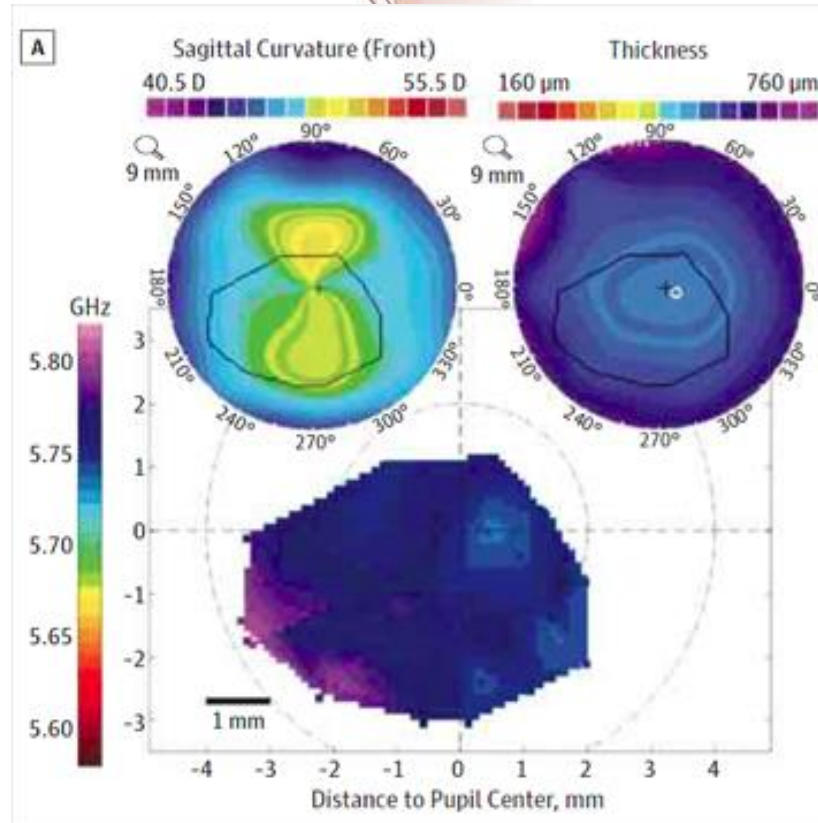
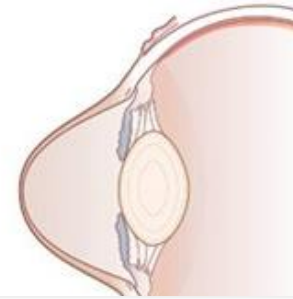


# Elastography of human cornea

healthy cornea



cornea with advanced keratoconus



6

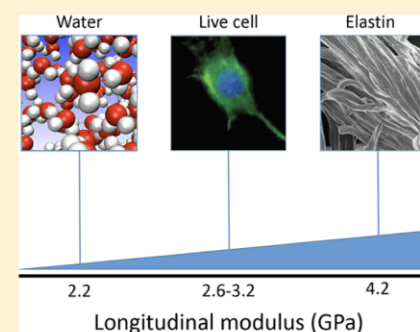
## Brillouin Light Scattering: Applications in Biomedical Sciences

Francesca Palombo<sup>\*,†</sup> and Daniele Fioretto<sup>‡</sup>

<sup>†</sup>School of Physics and Astronomy, University of Exeter, Stocker Road, EX4 4QL Exeter, U.K.

<sup>‡</sup>Department of Physics and Geology, University of Perugia, via Alessandro Pascoli, I-06123 Perugia, Italy

**ABSTRACT:** Brillouin spectroscopy and imaging are emerging techniques in analytical science, biophotonics, and biomedicine. They are based on Brillouin light scattering from acoustic waves or *phonons* in the GHz range, providing a nondestructive contactless probe of the mechanics on a microscale. Novel approaches and applications of these techniques to the field of biomedical sciences are discussed, highlighting the theoretical foundations and experimental methods that have been developed to date. Acknowledging that this is a fast moving field, a comprehensive account of the relevant literature is critically assessed here.



nature | methods

REVIEW ARTICLE

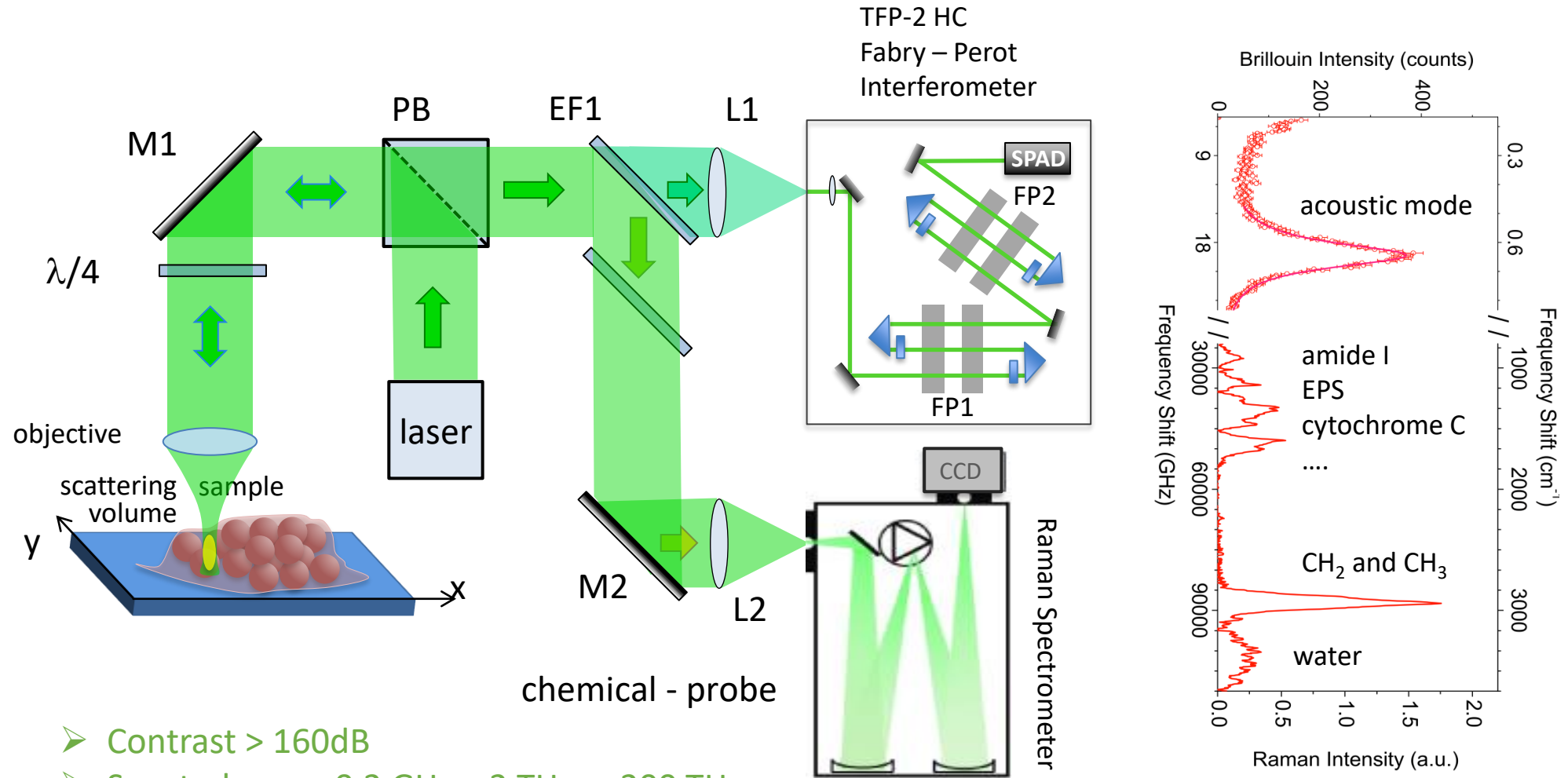
<https://doi.org/10.1038/s41592-019-0543-3>

## Brillouin microscopy: an emerging tool for mechanobiology

Robert Prevedel<sup>1,2,3\*</sup>, Alba Diz-Muñoz<sup>1\*</sup>, Giancarlo Ruocco<sup>4,5</sup> and Giuseppe Antonacci<sup>4,6</sup>

# Micro Brillouin & Micro Raman @ Perugia

PHYSICAL REVIEW X 7, 031015 (2017)

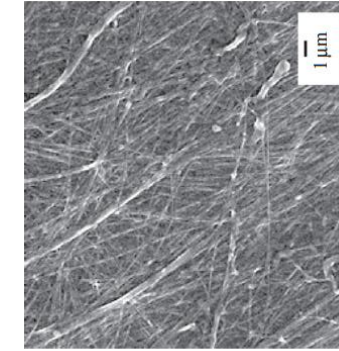
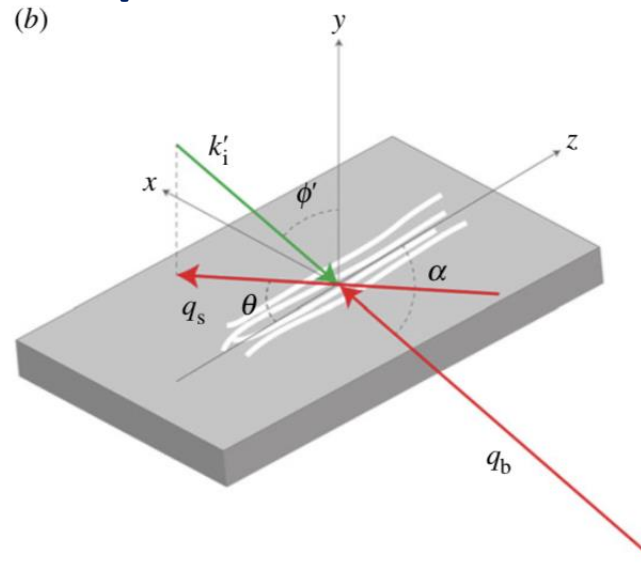
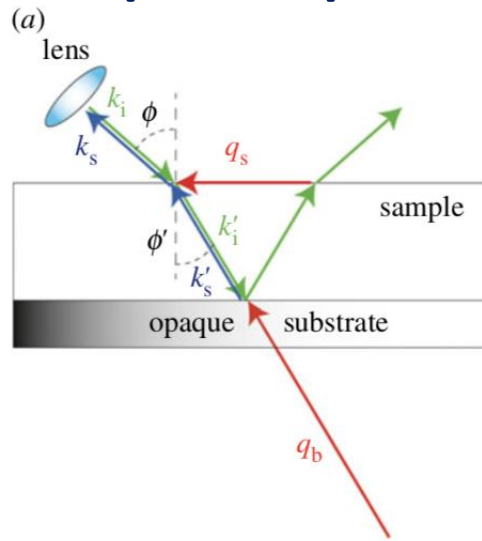


- Contrast > 160dB
- Spectral range 0.2 GHz – 2 THz +>200 THz
- Resolution better than 0.2 GHz
- Time for a measurement 0.5s - minutes

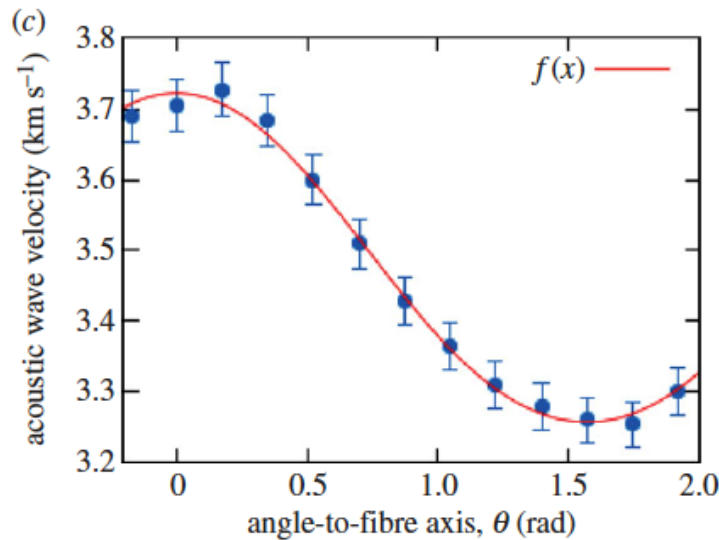


# Biomedical applications: Tissues

## Anisotropic samples: fibrous proteins of the extracellular matrix



type I collagen in rat tail tendon



$$V_{\text{T}}^2(\theta) = \frac{1}{\rho} \left( \frac{(c_{11} - c_{12})}{2} \sin^2 \theta + c_{44} \cos^2 \theta \right)$$

$$V_{\text{L}}^2(\theta) = \frac{1}{2\rho} \left\{ c_{11} \sin^2 \theta + c_{33} \cos^2 \theta + c_{44} + \left\{ [(c_{11} - c_{44}) \sin^2 \theta + (c_{44} - c_{33}) \cos^2 \theta]^2 + 4(c_{13} + c_{44})^2 \sin^2 \theta \cos^2 \theta \right\}^{1/2} \right\}$$

# Biomedical applications: Tissues

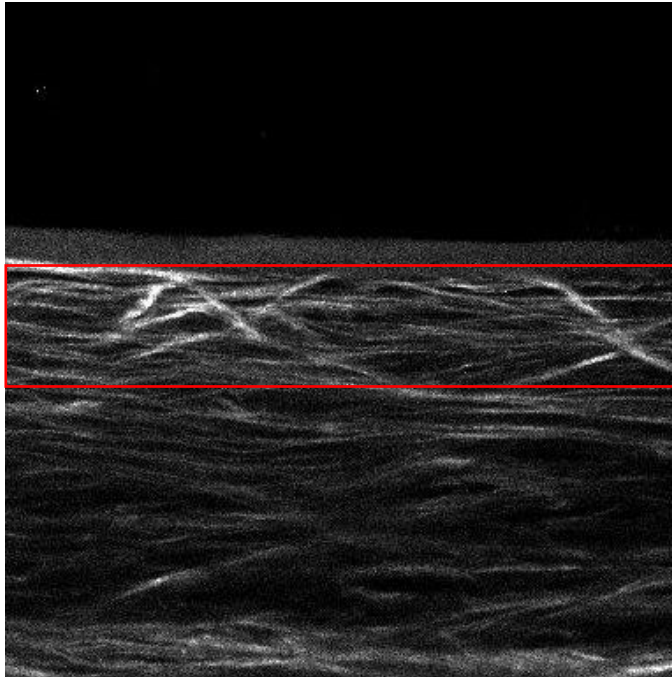
## Anisotropic samples: fibrous proteins of the extracellular matrix

sample	elastic coefficients (GPa)		elastic moduli (GPa)		Poisson's ratios		tan( $\delta$ )
	$c_{33}$	$c_{11}$	$E_{  }$	$E_{\perp}$	$\sigma_{13}$	$\sigma_{12}$	
collagen	$18.6 \pm 0.1$		$10.2 \pm 0.3$		$0.43 \pm 0.01$		$0.063 \pm 0.01$
	$14.3 \pm 0.1$		$8.3 \pm 0.3$		$0.32 \pm 0.02$		
	$3.2 \pm 0.1$		$3.2 \pm 0.1$				
	$8.0 \pm 0.1$		$10.9 \pm 0.5$				
	$9.7 \pm 0.2$						
elastin	$11.5 \pm 0.2$		$6.1 \pm 0.4$		$0.40 \pm 0.02$		$0.062 \pm 0.01$
	$10.4 \pm 0.1$		$5.3 \pm 0.6$		$0.40 \pm 0.06$		
	$1.9 \pm 0.2$		$1.9 \pm 0.2$				
	$6.6 \pm 0.2$		$8 \pm 1$				
	$6.8 \pm 0.3$						
ligament	$10.8 \pm 0.1$						$0.059 \pm 0.01$
	$10.8 \pm 0.1$						
cartilage	$13.4 \pm 0.2$						$0.080 \pm 0.01$
	$13.4 \pm 0.2$						

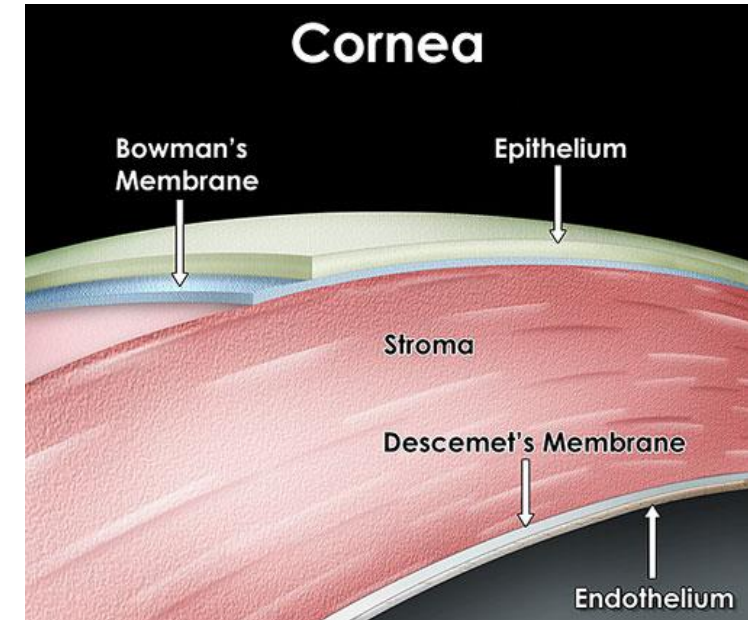
# Elastography of human cornea

## Morphological information on collagenous tissues by SHG microscopy

SHG-imaging **Healthy Cornea**



*Excitation wav.: 840 nm*  
*Detection wav.: 420 nm*  
*Detection type: F-SHG*  
*Pixel dwell time: 20  $\mu$ s*  
*FOV: 300  $\mu$ m*  
*Sectioning: Sagittal*



<http://www.nkcf.org/how-the-human-eye-works/>

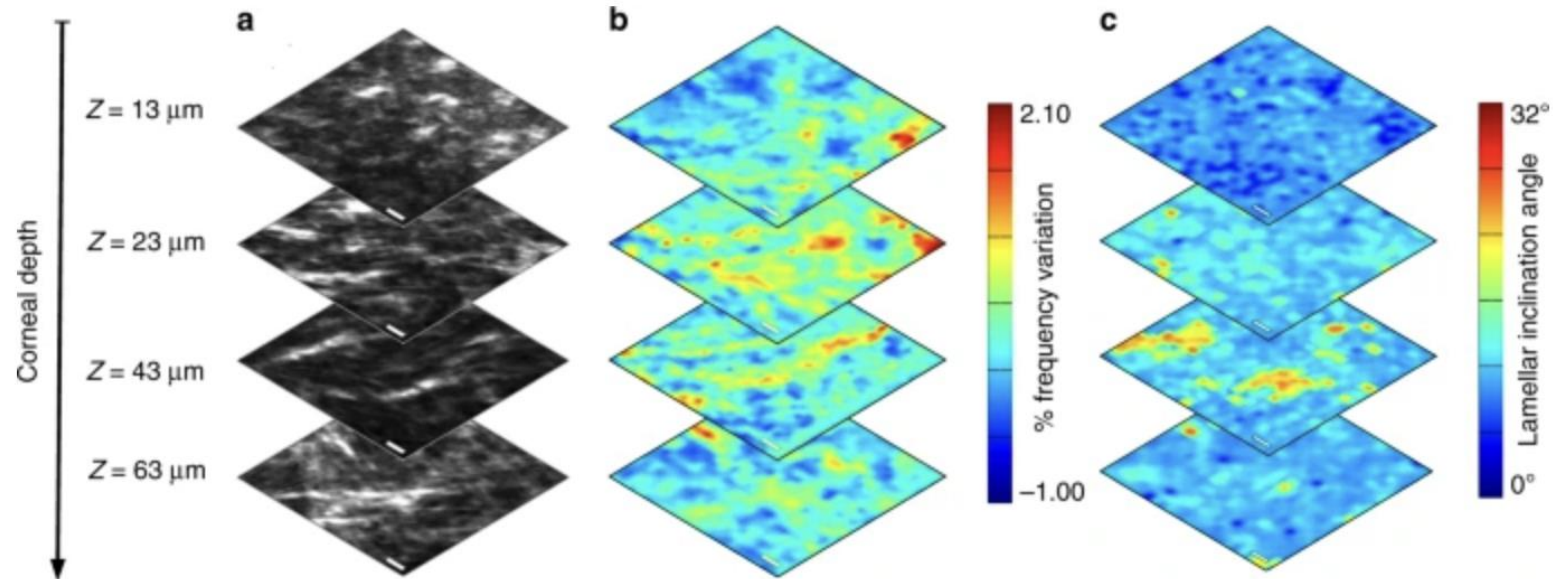
- The **sutural lamellae**, immediately below Bowman's membrane

R. Mercatelli et al. J. Biophoton. 10, 75-83 (2017)

# Elastography of human cornea

## Collagen morpho-mechanics: correlative SHG & Brillouin microscopy

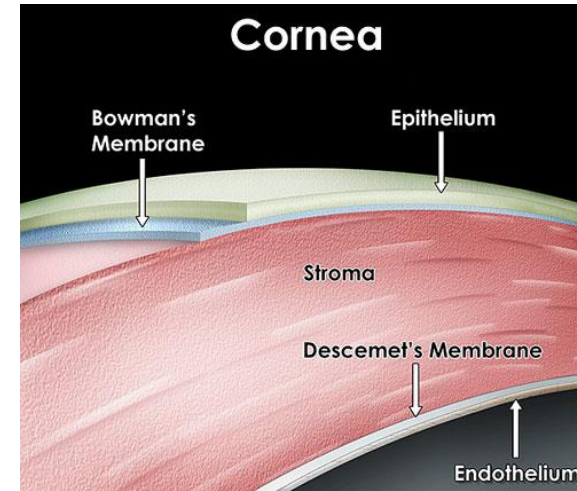
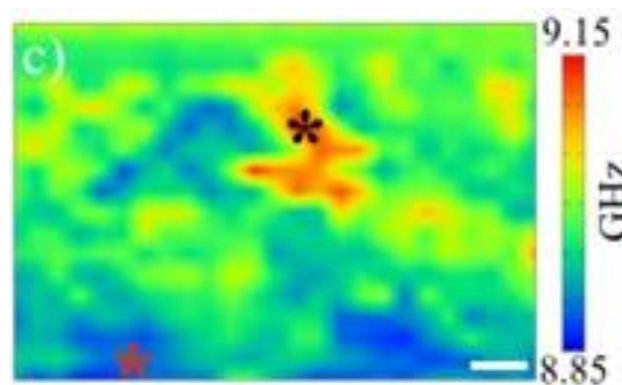
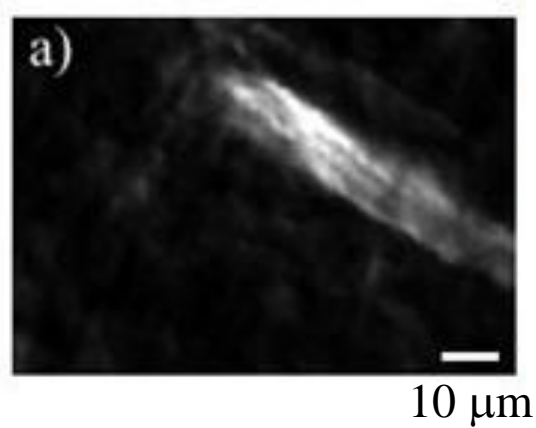
Fig. 3



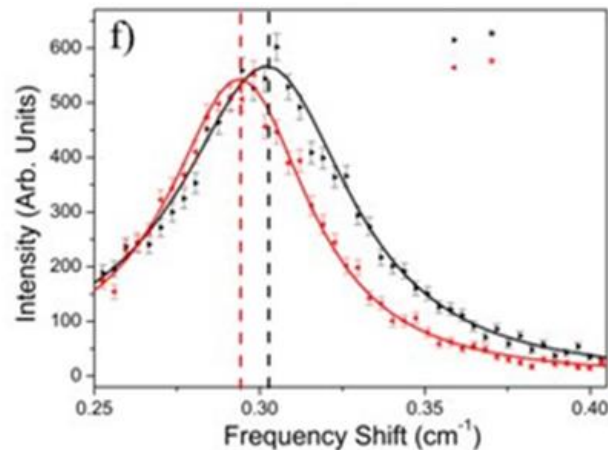
Correlative SHG-Brillouin axial optical sectioning analysis on corneal stroma. Comparison between (a) SHG images, (b) relative variations of Brillouin frequency and (c) lamellar inclination maps, acquired at the specified depths below Bowman's membrane. Scale bars: 10  $\mu\text{m}$

# Elastography of human cornea

## Collagen morpho-mechanics: correlative SHG & Brillouin microscopy



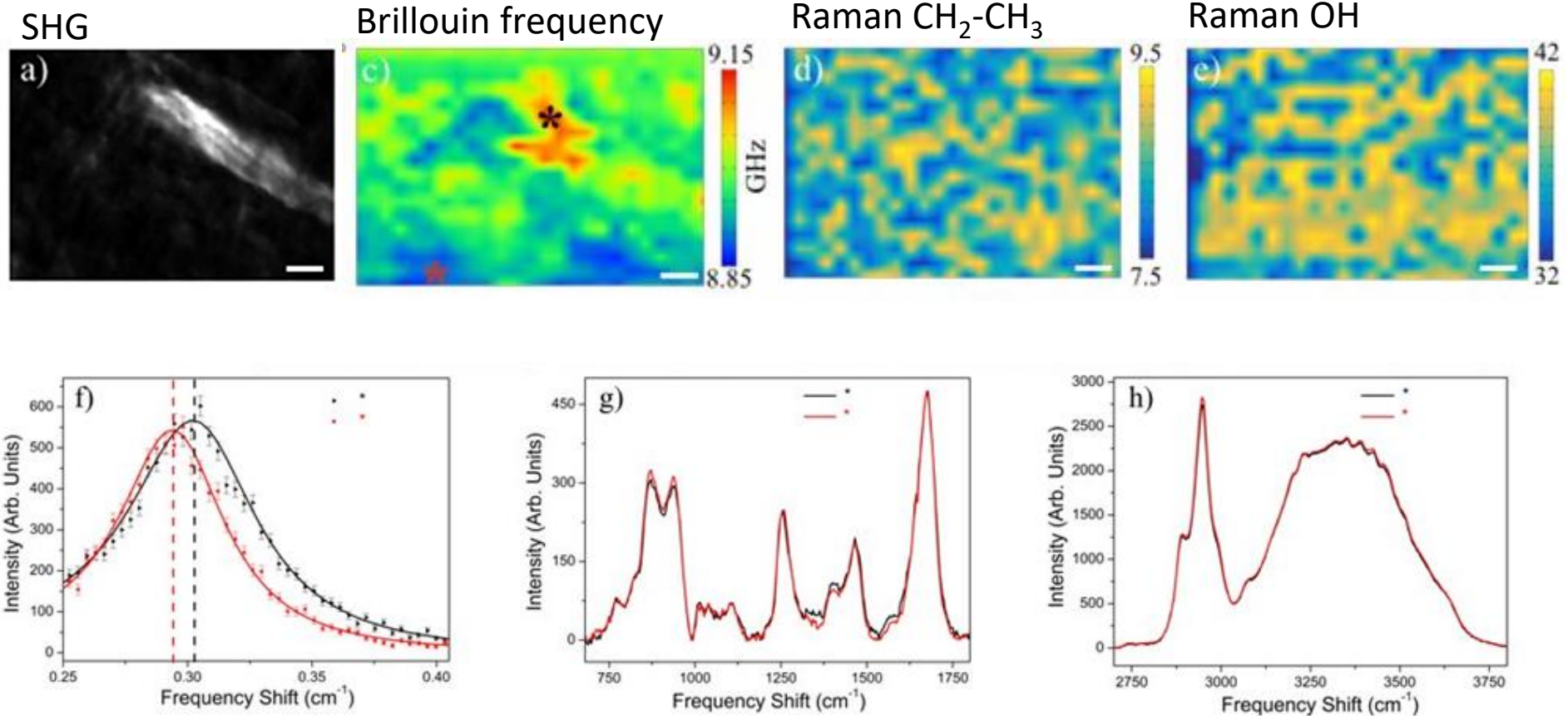
<http://www.nkcf.org/how-the-human-eye-works/>



The **heterogeneity in the stiffness** displays a striking conformity with the SHG signal highlighting the ability of Brillouin spectroscopy to detect individual sutural lamellae as an elastic modulation inside the tissue.

# Elastography of human cornea

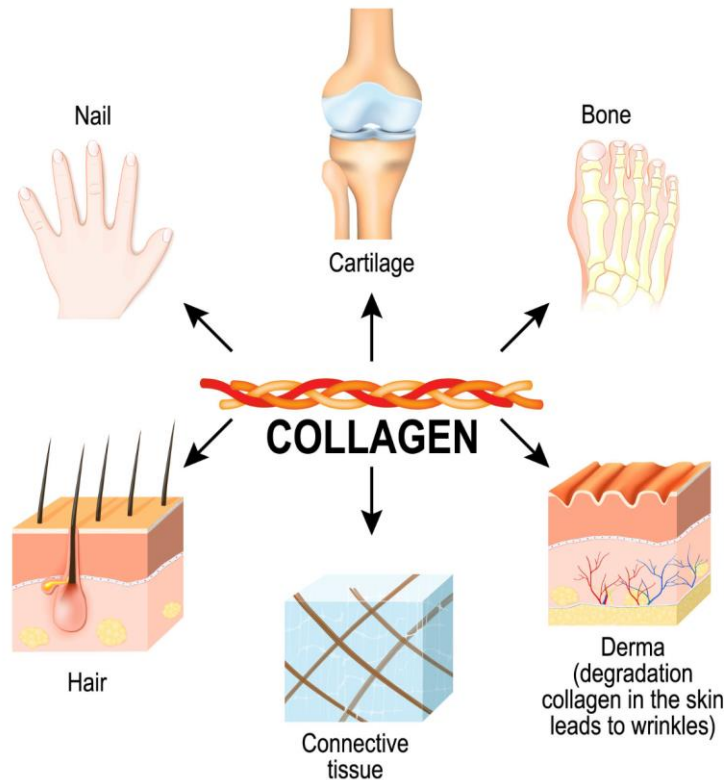
## Collagen morpho-mechanics: correlative SHG & Brillouin microscopy



The enhancement of the elastic modulus found in sutural lamellae has to do with morphological rather than biochemical factors.

# Basic questions: soft vs. hard, a matter of time

Gelatin (animal glue) as a model system in which the macroscopic physical properties can be manipulated to mimic all the relevant biological states of matter, ranging from the liquid to the gel and the glassy phase



The most ubiquitous structural protein

SCIENCE ADVANCES | RESEARCH ARTICLE 2020; 6 : eabc1937

## BIOPHYSICS

# Viscoelastic properties of biopolymer hydrogels determined by Brillouin spectroscopy: A probe of tissue micromechanics

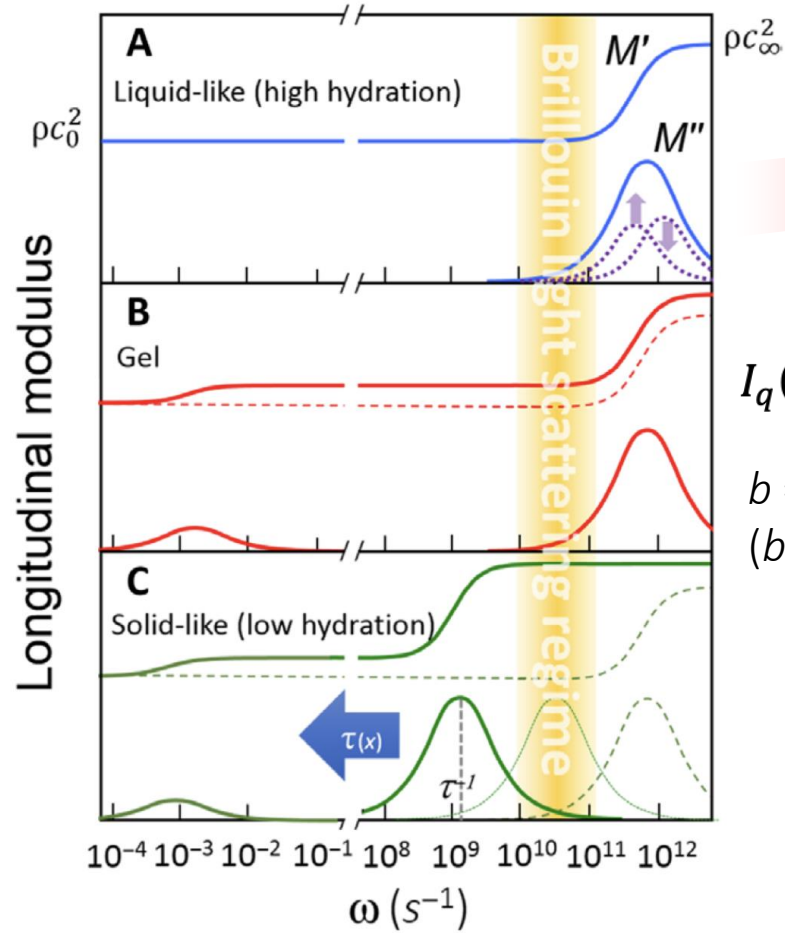
Michelle Bailey<sup>1</sup>, Martina Alunni-Cardinali<sup>2</sup>, Noemi Correa<sup>1</sup>, Silvia Caponi<sup>3</sup>, Timothy Holsgrove<sup>4</sup>, Hugh Barr<sup>5</sup>, Nick Stone<sup>1</sup>, C. Peter Winlove<sup>1</sup>, Daniele Fioretto<sup>2\*</sup>, Francesca Palombo<sup>1\*</sup>



Denaturated Type I Collagen

# Basic questions: soft vs. hard, a matter of time

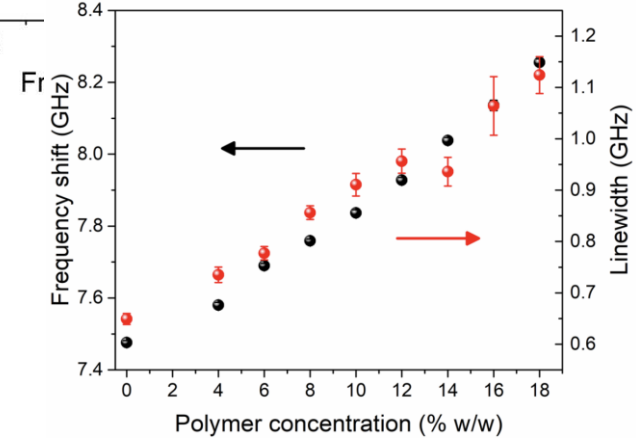
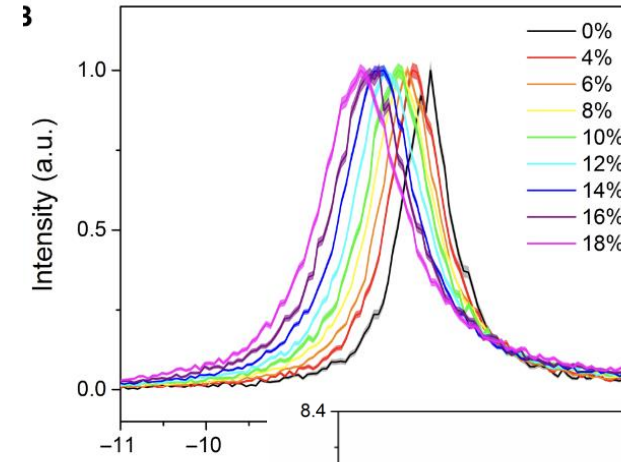
M. Bailey et al., Science Advances 6, eabc1937 (2020)



$$I_q(\omega) = I_0 \frac{\omega_B^2 \Gamma_B}{(\omega_B^2 - \omega^2)^2 - (\omega \Gamma_B)^2}$$

$$b = \Gamma / q^2$$

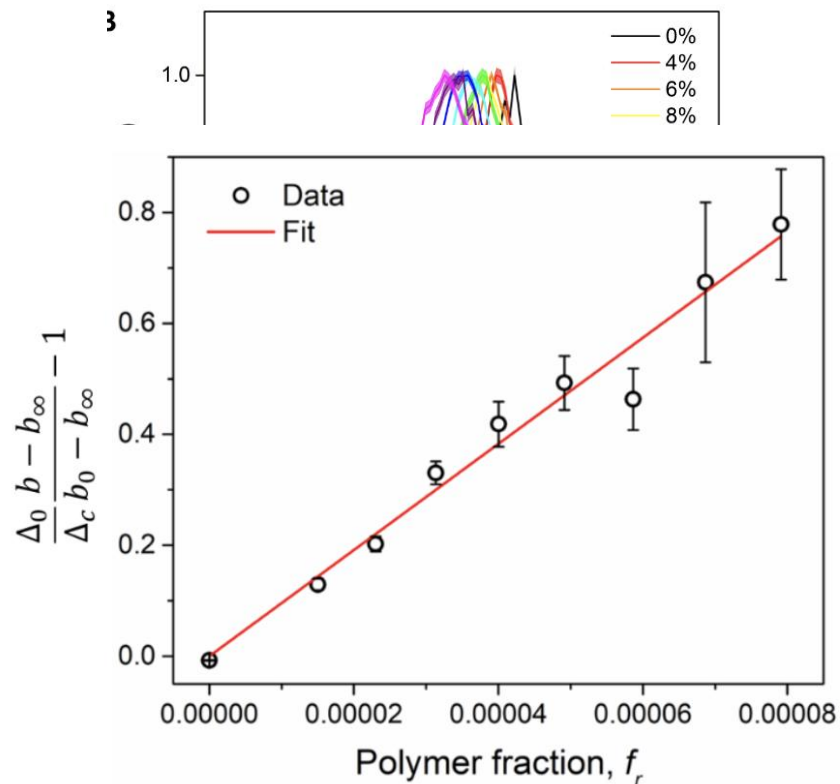
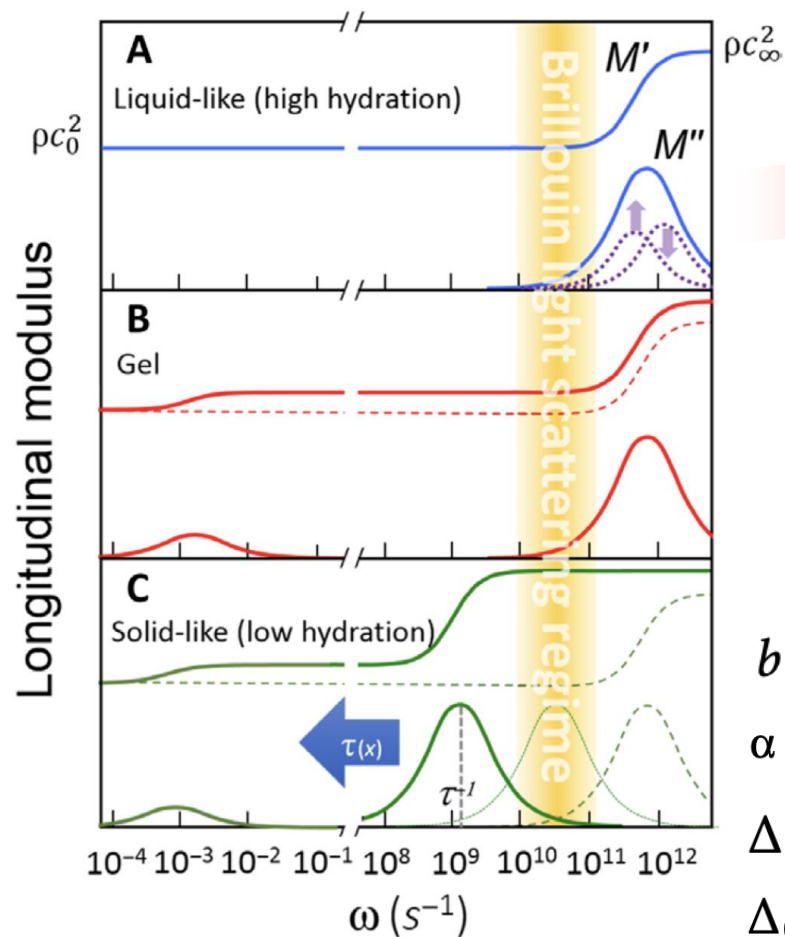
$$(b = \eta_L / \rho = M'' / \rho \omega)$$





# Basic questions: soft vs. hard, a matter of time

M. Bailey et al., Science Advances 6, eabc1937 (2020)



$$b = \Delta_c [\alpha \tau_h + (1 - \alpha) \tau_b] + b_\infty$$

$\alpha = f_r N_h$ , where  $f_r$  is the fraction of polymer-to-water

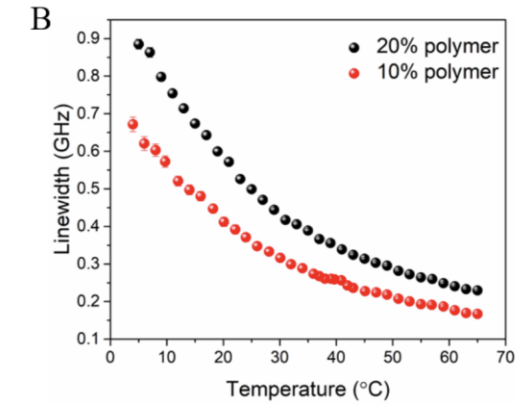
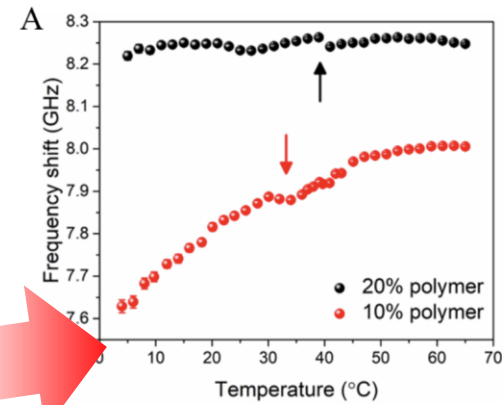
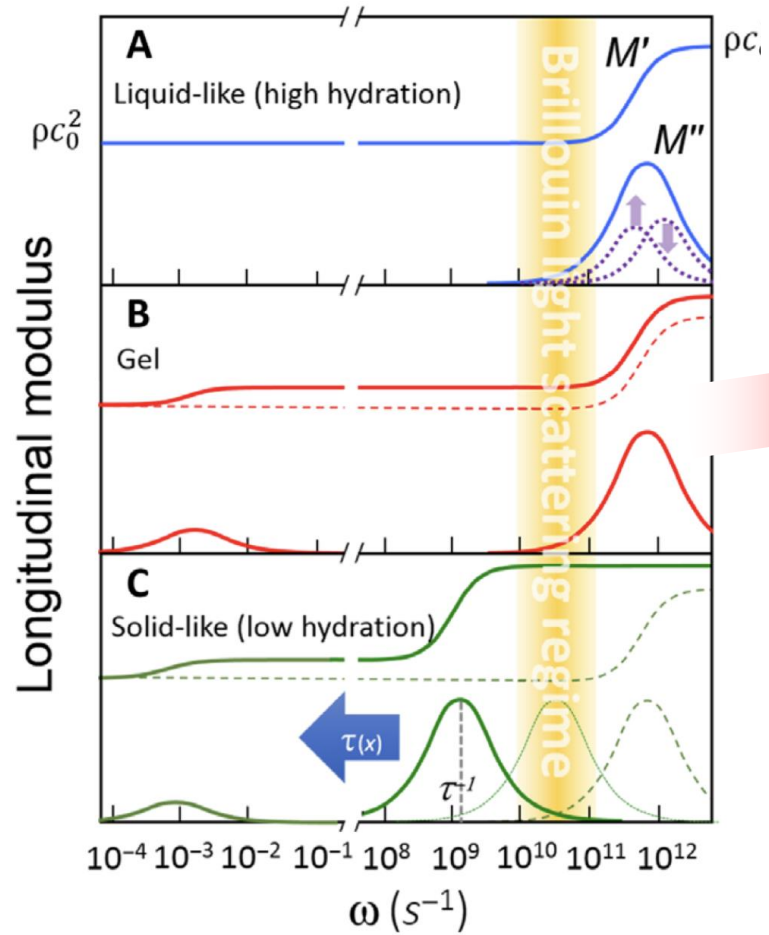
$$\Delta_c = c_\infty^2 - c_0^2$$

$$\frac{\Delta_0}{\Delta_c} \frac{b - b_\infty}{b_0 - b_\infty} - 1 = N_h(\epsilon - 1) f_r$$

$N_h = 10 \text{ k}$  → retardation parameter  $\epsilon = \tau_h / \tau_b = 1.9$

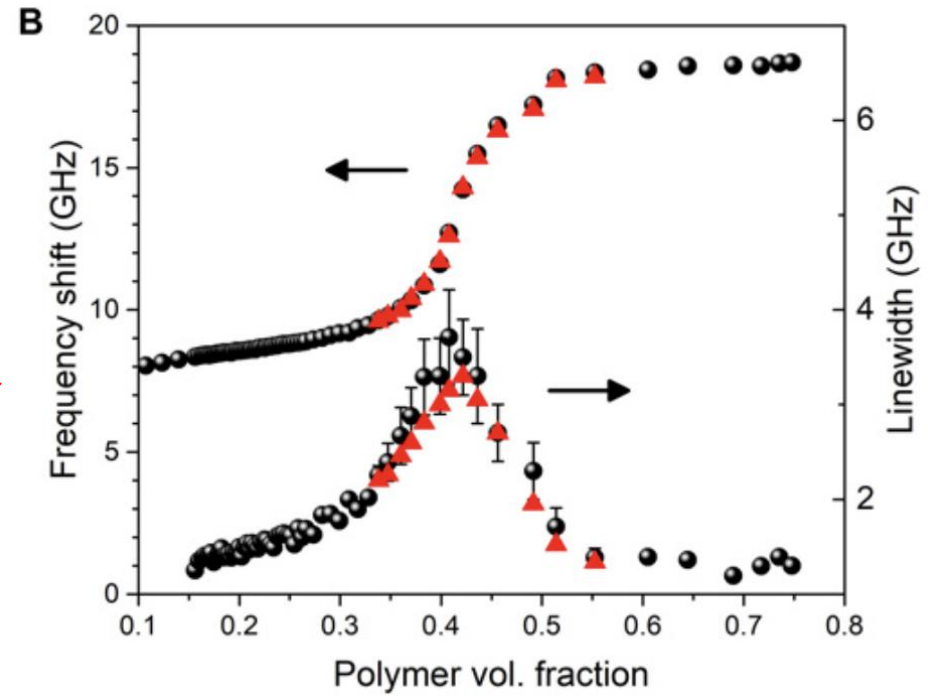
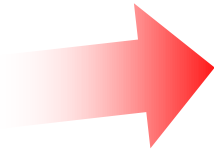
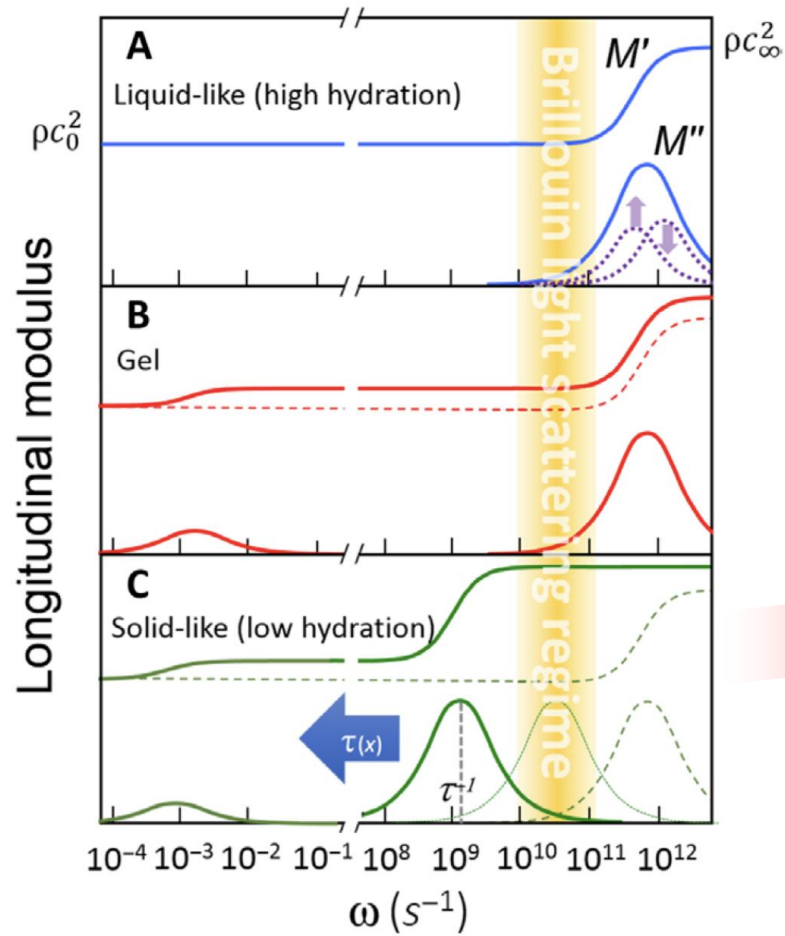
# Basic questions: soft vs. hard, a matter of time

M. Bailey et al., Science Advances 6, eabc1937 (2020)

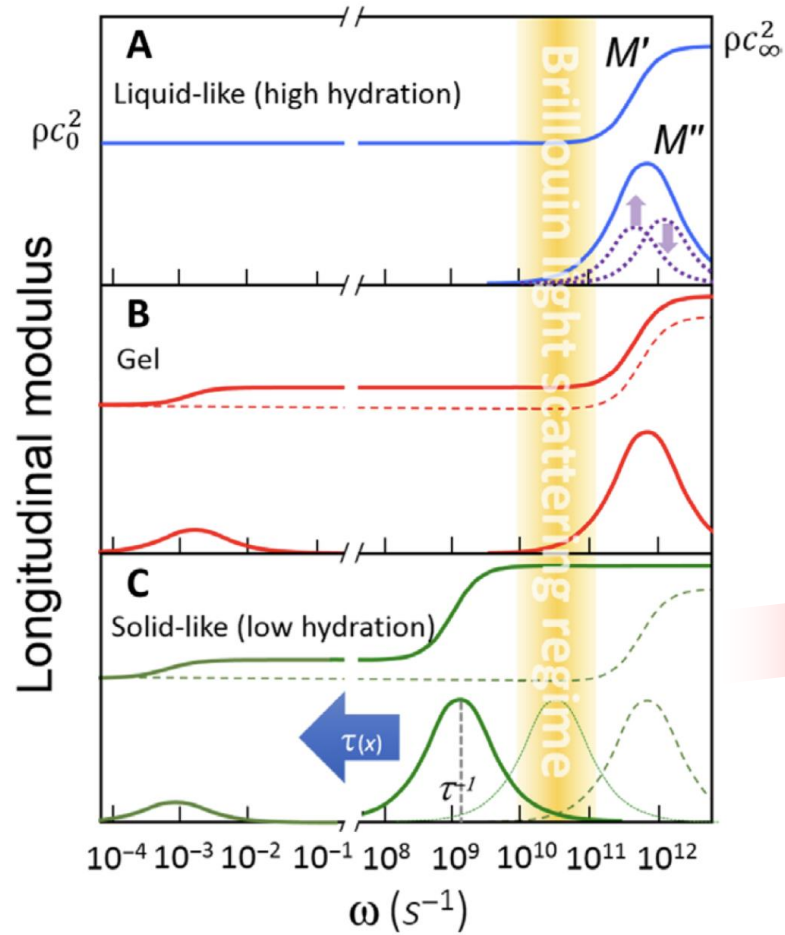


**Supplementary Figure s4.** Gel transition. Evolution of (A) frequency shift and (B) linewidth derived from Brillouin spectra of hydrogels as the temperature is reduced from 65 to 4-5 $^{\circ}C$ . Arrows indicate the gel transition.

# Basic questions: soft vs. hard, a matter of time

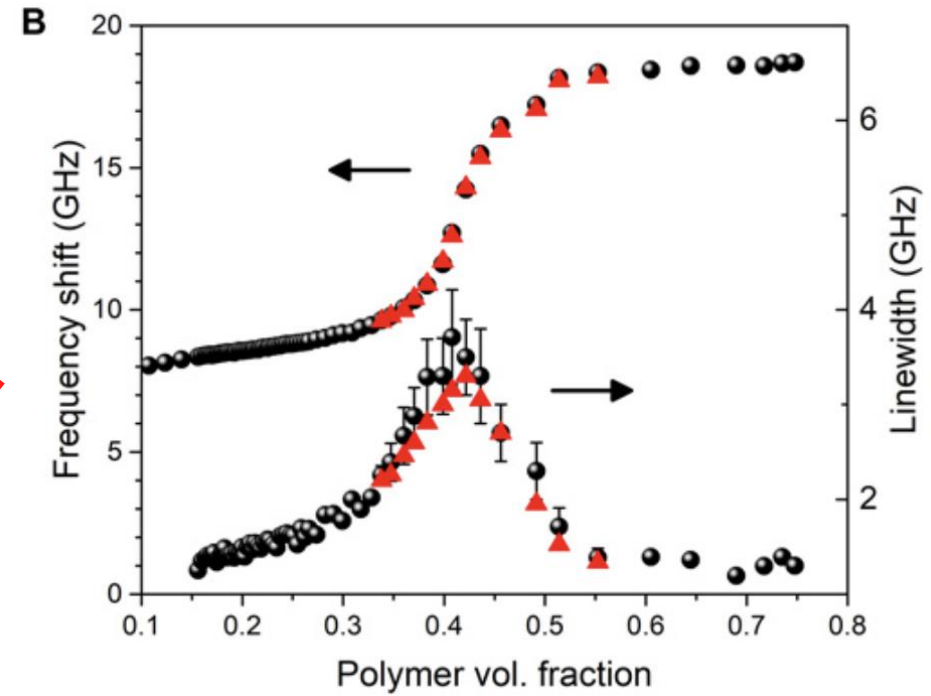
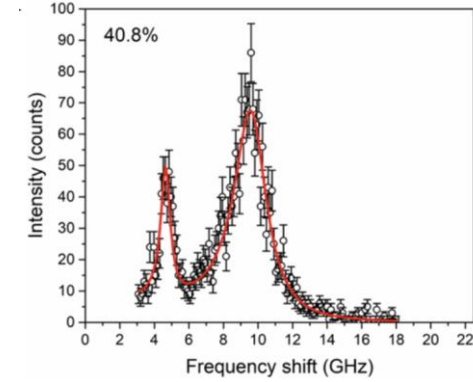


# Basic questions: soft vs. hard, a matter of time

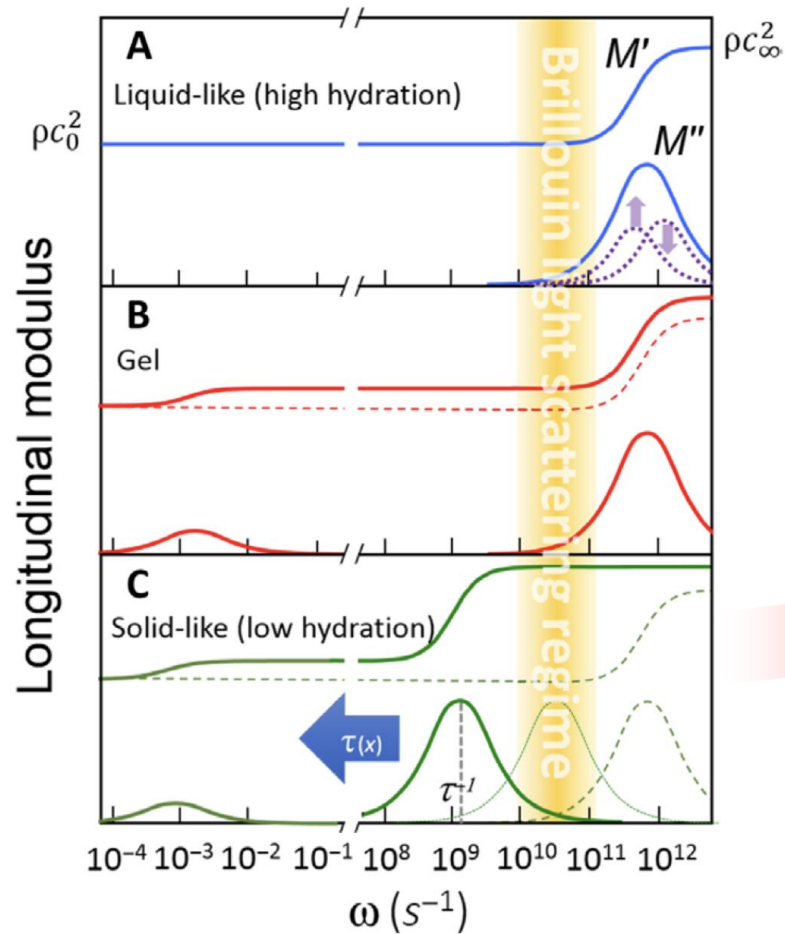


$$I_q(\omega) = \frac{I_0}{\omega} \Im \{ [M(\omega) / \rho - \omega^2 / q^2]^{-1} \}$$

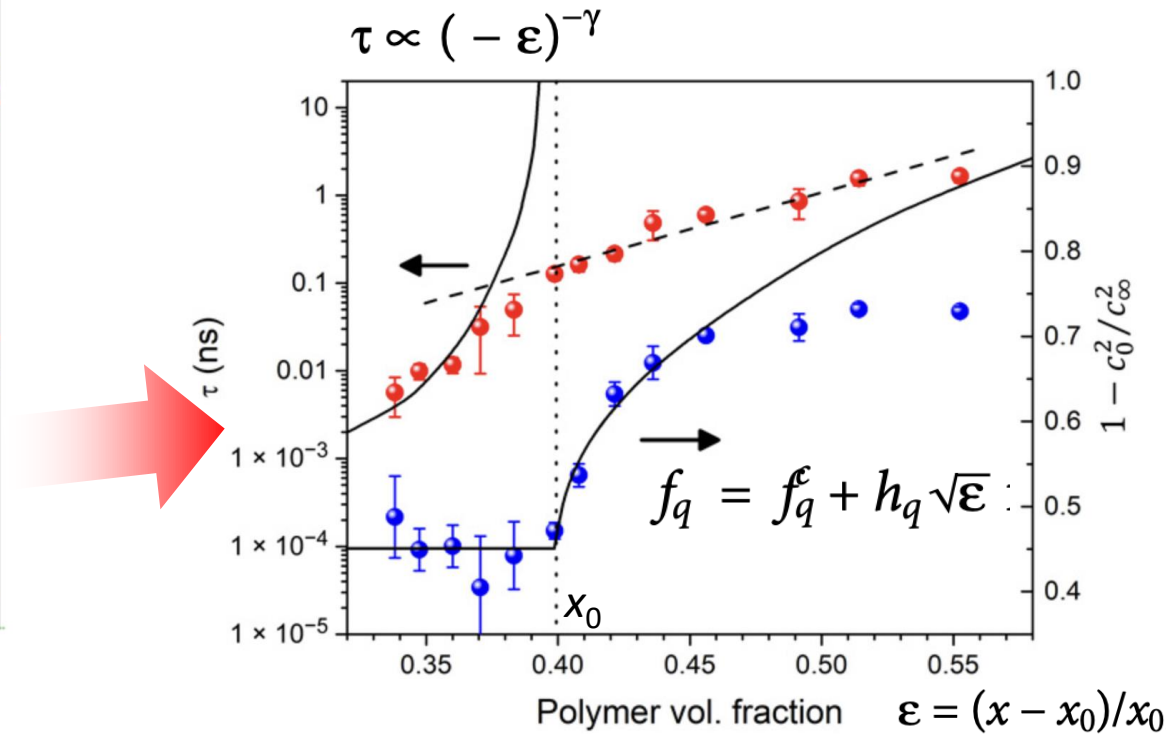
$$\frac{M(\omega)}{\rho} = c_\infty^2 - \frac{c_\infty^2 - c_0^2}{[1 + (i\omega\tau)^2]^b}$$



# Basic questions: soft vs. hard, a matter of time



Signature of power law divergence of the relaxation time and square root singularity of the non-ergodicity parameter (+ secondary relaxations) @ a critical polymer concentration  $x_0$



MCT is able to capture the early stage structural arrest mechanism, even in animal glue

# Summary

Brillouin light scattering is an “ancient” technique that is gaining interest as an optical elastography technique to provide a non-destructive, non-contact probe of the micromechanics of biological matter

Biological matter is a challenging workbench for testing a number of fundamental issues, such as the extent of acoustic modes in disordered matter, the role of heterogeneity in the propagation and attenuation of acoustic modes, the dynamics of hydration water and the nature of the structural arrest and of the glass transition

# Thank You!

*Martina Alunni Cardinali*  
*Silvia Corezzi*  
*Sara Mattana*  
*Maurizio Mattarelli*  
*Alessandra Anna Passeri*



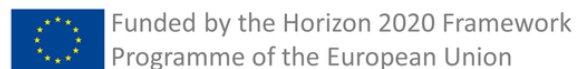
*Francesca Palombo*  
*Nick Stone*  
*Peter Winlove*



*Silvia Caponi*  
*Lucia Comez*



*Filippo Scarponi*



M.A.C., M.M. and D.F. were supported by the **CARIT** Foundation Project, call 02/2021 ( project code: FCTR21UNIPG).